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Review

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Effects of pulsed electromagnetic fields on articular hyaline cartilage: review of experimental and clinical studies

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Abstract

Osteoarthritis (OA) is the most common disorder of the musculoskeletal system and is a consequence of mechanical and biological events that destabilize tissue homeostasis in articular joints. Controlling chondrocyte death and apoptosis, function, response to anabolic and catabolic stimuli, matrix synthesis or degradation and inflammation is the most important target of potential chondroprotective treatment, aimed to retard or stabilize the progression of OA. Although many drugs or substances have been recently introduced for the treatment of OA, the majority of them relieve pain and increase function, but do not modify the complex pathological processes that occur in these tissues. Pulsed electromagnetic fields (PEMFs) have a number of well-documented physiological effects on cells and tissues including the upregulation of gene expression of members of the transforming growth factor β super family, the increase in glycosaminoglycan levels, and an anti-inflammatory action. Therefore, there is a strong rationale supporting the in vivo use of biophysical stimulation with PEMFs for the treatment of OA. In the present paper some recent experimental in vitro and in vivo data on the effect of PEMFs on articular cartilage were reviewed. These data strongly support the clinical use of PEMFs in OA patients.

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1. Introduction

Hyaline articular cartilage is an avascular and specialized functional tissue with low cellularity, high water content, and a dense extracellular matrix (ECM) [26]. The tissue-specific mechanical properties of articular cartilage are dependent on the ECM structure and composition, which accounts for about 90% of cartilage wet weight, and is mainly composed of collagen type II, proteoglycans (PG) (in particular, aggrecan, hyaluronic acid), cations and water [45]. The complex structure of articular cartilage enables this tissue to perform its biomechanical role but appears to hinder repair, as lesions without further surgical treatment often progress into longterm degeneration and osteoarthritis (OA) [17,26]. Even in the absence of injuries, accidents and other joint traumas, articular spontaneous degeneration occurs and prevalence studies indicate that the majority of people over the age of 65 have some form of OA [48].

OA is characterized by a degeneration of hyaline articular cartilage. The breakdown of the cartilage matrix leads to the development of fibrillations, clefts and ulcerations and the disappearance of the full-thickness surface of the joint. This process is accompanied by bone changes with osteophyte formation and thickening of the subchondral bone [43]. Even if changes in the subchondral bone resulting in loss of its stock absorbing capacity could transfer the stress of loading directly to the articular cartilage with secondary changes in the cartilage, OA is usually considered to be a primary disorder of chondrocyte proliferation and function with secondary changes in bone and it is often associated with an inflammatory response [16,30]. Chondrocytes are the single cellular component of hyaline cartilage and are responsible for matrix synthesis and turnover, while the state of the matrix has a

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direct influence on chondrocyte function. The number of chondrocytes, their rate of proliferation, metabolic activity and ability to respond to various stimuli are inversely related to the age of the organism [38,47].

Moreover, cytokines are considered to be an important link in OA since they are produced by cells present in the OA joints and because they are responsible, at least in part, for the changes seen in cartilage damage, synovial membrane, subchondral bone and osteophyte formation [41]. Local release of catabolic cytokines and enzymes such as interleukin 1 β (IL-1 β), tumor necrosis factor- α (TNF- α), interleukin 6 (IL-6), metalloproteinases (MMP), aggrecanases that is high in OA in response to tissue damage, and inflammation cause a depletion of glycosaminoglycans (GAGs) and suppress type II collagen synthesis [41,45]. Blockade of these cytokines by natural antagonists in OA cartilage, where they are overexpressed, can up-regulate gene expression of the matrix molecules and enhance matrix repair [36]. Furthermore, anabolic cytokines, such as insulin-like growth factor-I (IGF-I), TGFβ-1, inhibit the catabolic effects of pro-inflammatory cytokines [41] and may stimulate useful synthetic processes.

So, controlling chondrocyte death, proliferation, function, response to anabolic and catabolic stimuli, matrix synthesis, matrix degradation and joint inflammation is the most important target of a potential chondroprotective treatment, that is to say a therapy that retards or stabilizes the progression of established OA by altering the underlying pathological processes [1].

Many drugs or substances have been recently introduced for the treatment of OA including cyclooxyganes inhibitors, hyaluronic acid, chondroitin sulfate, and glucosamine sulfate [5,25,53,62]; however the majority of them can relieve pain and increase function, but do not modify the complex pathological processes that occur in these tissues, which are unable to balance undergoing catabolic and anabolic pathways [34]. In addition, such therapy for OA is unlikely to have a direct effect at the subchondral bone level [42,54].

Pulsed electromagnetic fields (PEMFs) have a number of well-documented physiological effects on cells and tissues including the upregulation of gene expression of members of the TGF β super family, the preservation of ECM integrity of cultured cartilage explants, the increase in GAG levels in embryonic and immature cartilage and in an experimental model of decalcified bone matrix-induced endochondral ossification [2,11,24,32,33,56]. An anti-inflammatory action has also been shown because of a direct effect on adenosine A2a receptors on cell membranes [63]. Several anti-inflammatory drugs are mediated via adenosine receptors and the modulation of the adenosine-receptor-mediated pathway may offer novel methods for treatment of inflammation in the presence of joint diseases [6].

Therefore, there is a strong rationale supporting the in vivo use of biophysical stimulation with PEMFs for the treatment of OA.

In the present paper some experimental (in vitro and in vivo) and clinical studies on the effect of PEMFs on hyaline

articular cartilage will be summarized. We searched the English language literature of the MEDLINE database, for the period January 1990 to December 2004 (keywords or title words: PEMFs and cartilage/chondrocytes/osteoarthritis). Articles were included in the review if they were related to the use of PEMFs on hyaline articular cartilage tissue or cells. The search included in vitro, animal and human studies. We excluded reviews and papers with not available full manuscripts. Finally, we excluded papers published before 1990 in an attempt to examine the most up-to-date methodology and outcome measures. We were left with six in vitro, two in vivo and five clinical papers.

2. In vitro studies: PEMF effects on cartilage cell and tissue cultures

The studies summarized in Table 1 on the in vitro effect of PEMFs on hyaline articular chondrocytes and articular cartilagineous tissue have appeared in the literature over the last 10 years [13–15,22,44,52]. They considered different pathogenetic aspects (chondrocyte proliferation, ECM synthesis, secretory activity and inflammation).

More precisely, PEMFs were tested in human and animal monolayer chondrocyte cultures and tissue explants and their effects were investigated by different methodologies. Conflicting observations have been reported and some studies demonstrated a significant effect of PEMFs in increasing articular chondrocyte proliferation [13,44,52], ECM synthesis and PG content in cartilage tissue explants [14] while others demonstrated that PEMFs had no effect on articular chondrocyte GAG synthesis [52].

Some authors also investigated: 1) the role of serum (fetal bovine serum, FBS) in the culture medium, that is to say the availability of growth factors [44]; 2) the contemporaneous administration of anabolic (IGF-1) and pro-inflammatory (IL- 1β) cytokines to PEMF stimulation [14,15,22]; 3) the dependence of the PEMF proliferative effects on cell density [13]. Therefore, these studies also permitted testing the PEMF mechanism of action and the therapeutic effect in conditions that simulate an OA inflammatory conditions in vitro. Briefly, it was shown that: 1) the proliferative response of chondrocytes to PEMF exposure is dependent on the amount of serum in the culture medium (0.5 and 10%) [44]; 2) the proliferative response to PEMFs is inversely correlated to the cell density and is strictly growth-stage dependent [13]; 3) PEMFs increased the anabolic effect of IGF-I on cartilaginous bovine explants, and PG synthesis was significantly improved by the PEMF stimulation independently of the absence or presence of serum [44]; 4) when IL-1 β was used in vitro to induce cartilage degradation PEMFs stimulated PG synthesis that completely compensated for the IL-1 β dependent inhibition of PG synthesis, thereby restoring its basal concentration level [14,22].

Of particular interest, the results of these studies demonstrate that the effect of PEMFs depend on the in vitro model

390 Table 1

Main in vitro studies on chondrocyte proliferation and ECM synthesis in PEMF stimulated and not stimulated cell and tissue cultures from articular hyaline cartilage (for the period January 1990 to December 2004)

Model	Stimulation	Main results	References
Human articular	Frequency 75 Hz	PEMFs significantly increased proliferation following 9 and 18 h of exposure in	[13]
chondrocytes at low and high	Intensity 2.3 mT	high and low density conditions.	
density	Pulse duration 1.3 ms	PEMFs significantly increased proliferation during the first 3 days of culture in low	
	Exposure time: 1, 6, 9, 18 h and continuous exposure for 3 and 6 days	density conditions. The exposure to PEMFs resulted in a significant increase of proliferation versus control cultures in the first 2 days	
Bovine articular cartilage explants both in basal conditions and in the presence of IL-1 β	Frequency: 75 Hz	PG synthesis and the residual PG tissue content were significantly higher in PEMF-exposed explants than in controls. II-1β induced both a reduction of PG synthesis and an increase in PG release which resulted in a net loss of tissue PG content. In IL-1 treated explants, PEMF increased PG synthesis without modifying PG release.	[14]
	Intensity: 2.3 mT		
	Pulse duration: 1.3 ms		
	Treatment length: 24 h		
Human nasal and articular monolayer chondrocyte cultures in the absence and presence of serum	Frequency: 75 Hz	Significant increase in proliferation (3H-thymidine incorporation) in cultures [exposed to PEMFs in the presence of serum whereas no effects were observed in serum-free conditions.	[15]
	Intensity: 2.3 mT		
	Pulse duration: 1.3 ms		
	Treatment length: 6, 12, 18, 24 and 30 h		
Bovine articular chondrocyte monolayers cultures and bovine articular cartilaginous tissue explants in the absence and presence of serum and IGF-I	Frequency: 75 Hz	In cartilage explants, PEMF stimulation significantly increased PG synthesis both in the absence and in the presence of serum. Similarly, IGF-I increased PG synthesis in a dose-dependent manner both in the absence and presence of serum. At all doses of IGF-I, the combined effects of the 2 stimuli resulted additive. No effect was observed on medium PG release. Also in chondrocyte monolayers IGF-I	[44]
	Intensity: 1.5 mT		
	Pulse duration: 1.3 ms		
	Treatment length: 24 h	stimulated PG synthesis in a dose-dependent manner, both in the absence and presence of serum, however this was not modified by PEMF exposure.	
Human articular osteoarthritic chondrocytes in alginate and the absence and presence of IL-1 beta	Pulsed signal therapy	IL-1 beta induced marked cellular damage observed by TEM analysis and a	[22]
	(PST)	significant decrease of PG levels. PST stimulation leads to restoration of cell	
	Frequency: < 30 Hz	structure and of PG production.	
	Intensity: 10–20 G		
	Pulse duration: 6/ ms		
	a h/day for 72 h		
Human articular cartilage cells	5 II/day IOI 72 II Frequency: 6 4 Hz	The stimulation promoted cell proliferation but did not enhance GAG synthesis	[52]
	Intensity: 0.4 mT	The sumulation promoted cent promeration out the not enhance GAG synthesis	[32]
	Pulse width: 230 us		
	Burst width: 76 ms		
	Treatment length: 5 days		
	engin o duys		

adopted (monolayer chondrocyte cultures versus tissue explants), the presence of growth factors in the microenvironment, and environmental constrictors.

3. In vivo studies: PEMF therapeutic efficacy on OA lesions

Because subchondral bone, bone marrow, synovial cells, chondrocytes and synovial fluid all contribute to the development of OA and to the healing of defects of articular cartilage, the use of animal models is essential both to understanding the process of repair and assessing the value of new therapeutic regimens [55]. Many techniques have been employed by researchers to create secondary OA lesions in animals and especially in rabbits, by means of surgical interventions that cause mechanical instability of the knee joint such as meniscectomy, section of anterior or posterior cruciate ligament (ACL, PCL), alone and in combination [29,31,35,45,50,51,64]. However, another animal model

which develops spontaneous and asymptomatic age-related OA of the knee is the Dunkin Hartley guinea pigs. The earliest histological signs of OA in Dunkin Hartley guinea pigs appear at 3 months of age in the medial tibial compartment and progress to moderate and severe degenerative changes at 1 year of age [27]. The resulting articular cartilage lesions resemble those found in humans and are also increased by body weight, mechanical load and posture [58].

To date, two in vivo experimental studies into the effect of PEMFs on OA have been performed in the aged Dunkin Hartley guinea pigs [11,21].

Ciombor et al. [11] utilized 12-month-old guinea pigs that were unstimulated for 6 months or stimulated for the same period 1 h/day with PEMFs (pulse-burst of 30 ms duration, repeated at 1.5 bursts per s with a peak magnetic field of 1.0 G, energy below 75 Hz). At the end of the experimental study the Authors excised both knees and studied the mid-portion of the tibial plateau by means of a histological/histochemical score (Mankin score with 0–6 points for cartilage structure; 0–3 points for chondrocyte abnormalities; 0–4 points for progressive decrease in safranin staining; 0-1 point for loss of tidemark integrity). Collagenase type II, stromelysin, IL-1 β , interleukin 1 receptor antagonist protein (IRAP) and TGFβ-1 were also studied by means of immunohistochemistry. Results showed that cartilage was thicker in the medial tibial plateau of guinea pigs stimulated with PEMFs in comparison with not stimulated animals, and the histological/ histochemical score was significantly lower in PEMF-treated animal than in Sham-treated animals. Moreover, PEMF treatment significantly reduced immunopositive cells to collagenase type II, stromelysin and IL-1 β , while the number of cells immunopositive for IRAP and TGF_β-1 was significantly increased. Ciombor et al. [11] suggested that PEMF stimulation of TGFB-1 might be responsible for the repair mechanism of action. TGFB-1 stimulates PG and collagen II synthesis and also acts as a natural inhibitor capable of directly counteracting pro-inflammatory cytokine production and activity [37,43].

Fini et al. [21] used the same animal model (12-month-old Dunkin Hartley guinea pig), which was stimulated with PEMFs for 3 months 6 h/day (frequency = 75 Hz, intensity of electromagnetic field = 1.6 mT and duty cycle = 1.3 ms). At the end of the study, the entire knee joints were investigated by means of microradiography, a histological/ histochemical grading score (Mankin modified by Carlsson with 0-8 points for cartilage structure; 0-3 points for chondrocyte abnormalities; 0-6 points for progressive decrease in toluidine blue staining; 0-1 point for loss of tidemark integrity) and cartilage and bone histomorphometry. Results of the study showed that PEMF-treated animals scored low, indicating a reduction in the progression of chondropathy in comparison with sham-treated animals. The results of medial tibia plateau had the highest histological grading scores in both experimental and control groups, indicating that this site was more susceptible to chondropathy. Regarding cartilage thickness (CT), a significantly higher value was found in the medial tibia plateaus of animals of the PEMF-treated group when compared to other measurement sites of the same group and to the CT value of the medial tibia plateaus of the animals of the Sham-treated Group. As far as bone was concerned, significantly lower values were observed in subchondral bone thickness for the PEMF-treated group in comparison to the sham-treated group when considering each measurement site.

These results have confirmed and extended the observations of Ciombor et al. [11] by showing that PEMFs preserve the morphology of articular cartilage and retard the development of OA lesions in the entire knee of aged osteoarthritic guinea pigs. An anti-inflammatory mechanism of action was also hypothesized on the basis of recent evidence regarding the chondroprotective effect of adenosine agonists selective to the A2a receptor and of the in vitro capability of PEMFs to increase the number of A2a adenosine receptors [63].

4. Clinical studies

Although the different animal models of OA have characteristics similar to the human disease, none of them has proven to be a true model of OA and therefore, any treatment has to be finally tested in clinical trials. PEMF stimulation is still under investigation for use in patients with OA [53]. However, even if different physical parameters and exposure times of stimulation were used, positive results were obtained in clinical studies [28,39,46,60,61].

In 1993, Trock et al. [60] performed a double-blind randomized clinical trial on patients with primary knee OA. Patients were treated with PEMFs (frequency: < 30 Hz; intensity: 10–20 G; 67 ms pulse phase duration) 30 min/day, three to five treatments per week for a total of 18 treatments in 1 month). At different time points, patients were evaluated for pain level, joint motion and tenderness. The actively treated group averaged 34% improvement in the mean value for each variable at each experimental point and 47% improvement by 1 month after treatment. Control patients averaged about 10% and 14% improvement at the same experimental points, respectively.

In 1994, the same authors [61] performed a similar study on the effect of PEMFs in the treatment of patients with knee and cervical spine OA. They observed a strong placebo effect and variability from patient to patient, but they confirmed the statistically significant improvement in pain score, daily activity, knee tenderness and motion for PEMF-treated patients with knee OA. PEMF-treated patients with cervical spine involvement always had a significant improvement by the end of treatment and at follow up.

In 2001, Pipitone and Scott [46] performed a randomized, double-blind, placebo-controlled study on the efficacy of PEMF stimulation in patients with symptomatic knee OA. At 6 weeks, patients were evaluated with different scores (Likert and Euro-Quality of Life). Paired analysis of the follow-up observations on each patient showed a significant improvement in the treated group with regards to pain and disability.

Also Jacobson et al. [28] and Nicolakis et al. [39] observed that PEMF stimulation was safe, reduced impairment in activities of daily life and improved knee function in patients with chronic knee pain due to OA.

5. Discussion and conclusion

In western countries the impact of OA on public health and the significant costs that musculoskeletal conditions generate will be of increasing burden [9]. Our understanding in the treatment of OA evolves as knowledge of the underlying pathophysiology of the condition improves. Previous concepts on OA pathogenesis focused only on the role of chondrocytes in the synthesis and degradation of the ECM. In fact, chondrocytes are the only cell type that constitutes articular cartilage and are responsible for tissue homeostasis, respond to injury and perform the cartilage remodeling process that characterizes OA [30]. More precisely, chondrocyte number, proliferation rate, synthetic and metabolic activity and growth factor responsiveness decrease with the advancing age and in the presence of OA [4]. Cell death and apoptosis during OA lesion progression have also been reported [30].

Newer concepts on OA pathogenesis are related to the role of inflammation that is now well accepted as a feature in OA [9]. Synovitis is common in advanced age involving infiltration of activated B cells and T lymphocytes and the expression of pro-inflammatory cytokines and chemokines is observed in patients with OA in the joints of OA patients and animals [7,23]. With regards to this, IL-1β, TNFα, IL-6, IL-18, IL-17 and leukemia inhibitory factor (LIF) appear to be more relevant to the disease [41,42]. These catabolic cytokines lead to the destruction of joint tissue by stimulating cartilage PG resorption, MMP synthesis and nitric oxide production [43,57]. The purine base adenosine has been shown to limit inflammation through receptor (i.e. A2a)-mediated regulation and suppressing pro-inflammatory cytokines synthesis (TNFa, IL-8, IL-2, IL-6). Adenosine has been reported to reduce inflammation and swelling in several in vivo models of inflammation and also in adjuvant-induced and septic arthritis in animals [8,12,57].

So, a therapy combining an anabolic effect on chondrocytes, a catabolic cytokine blockage, a stimulatory effect on anabolic cytokine production and one that is able to counteract the inflammatory process would be extremely useful for OA treatment.

In vitro studies showed that chondrocyte proliferation and matrix synthesis are significantly enhanced by PEMF stimulation, when investigating also the conditions affecting the PEMF action [13-15,22,44]. A part the importance of physical properties of the fields used (intensity, frequency, impulse amplitude, etc.) and the exposure time, the availability of growth factors, environmental constrictions and the maintenance of the native-cell matrix interactions seem to be fundamental in driving the PEMF-induced stimulation [13,15]. In particular, the interaction between cell membrane receptors and mitogens seems to be one of the molecular events affected by PEMFs [44]. These data are in agreement with results of in vivo studies with a decalcified bone matrixinduced endochondral ossification model and showing that the stimulation of TGF β -1 may be a mechanism through which PEMFs affect complex tissue behavior and through which the effects of PEMFs may be amplified [13]. In addition, PEMFs are reported to up-regulate mRNA levels for, and protein synthesis of, growth factors resulting in the synthesis of ECM proteins and acceleration of tissue repair [3].

As far as inflammation is concerned, IL-1 β is present in high amounts in OA cartilage and is considered to be one of the main catabolic factors involved in the cartilage matrix degradation associated with OA [23]. As previously mentioned, PEMFs in vitro were able to counterbalance efficiently the cartilage degradation induced by the catabolic cytokine [14,22].

Moreover, saturation-binding experiments demonstrated a significant increase in the adenosine A2a receptor density in human neutrophils treated with PEMFs [63]. Activation of adenosine A2a receptors seems to be associated with inhibition of the catabolic cytokines TNF α , IL-6 and IL-8 [6,57]. Although further studies are necessary to determine the direct

effect of PEMFs on chondrocyte A2a receptors, a similar mechanism of action could be hypothesized for OA joints on the basis of recent data showing the presence of A2a receptor on chondrocyte membrane, the response of chondrocytes to adenosine and the production of adenosine by chondrocytes [57].

Finally, studies of electrical phenomena in cartilage have suggested also a mechanical-electrical mechanism of action in vivo that resembles the one described in bone, appearing when cartilage is mechanically compressed and causing movement of fluid and electrolytes, leaving unneutralized negative charges in the proteoglycans and collagen in the cartilage matrix. These streaming potentials could work in cartilage and transduce mechanical stress to an electrical (or electromagnetic) phenomena capable of stimulating chondrocyte synthesis of matrix components [60]. The mentioned mechanisms seem to be active also in vivo, so that both in vivo studies performed so far in animals demonstrated important effects of PEMFs in controlling knee OA lesion progression [11,21]. These experimental results were also confirmed by clinical trials [28,39,46,60,61]. In the clinical use the control of the local environment by physical stimuli is achieved by exposing only the specific region/area of interest, and a therapeutic effect by can be activated by delivering locally the optimal effective dose. Thus, the treatment can be performed in the absence of systemic effects and complies with the principle of limiting iatrogenic side effects [20].

In conclusion, experimental and clinical studies suggest that PEMF stimulation would be a promising chondroprotective therapy for OA joints because of an action on chondrocyte metabolism that has been demonstrated in vivo by the enhancing of cartilaginous and subchondral bone tissue properties and in some clinical studies by the amelioration of clinical and radiographic observations. Future experimental studies may be aimed at clarifying the cellular and molecular events which are involved in the tissue response to PEMFs in innovative therapeutic strategies such as tissue engineering. Cell yield, proliferation/expansion and redifferentiation are the main phases of regenerative medicine that are particularly problematic in advanced aged and OA patients [4]. On the basis of the previously mentioned effect of PEMFs on chondrocyte cultures it could be hypothesized that stimulation might accelerate and ameliorate both expansion and redifferentiation. In this modern field of research, it would be important to use cell and tissue cultures from pathological joints. In vitro experimental data have demonstrated the importance of using pathological models to better simulate the clinical conditions [18,19,59], and differences between chondrocytes from healthy and OA joints have been reported [10,49]. Even if it was hypothesized that PEMF effects might be more evident in chondrocytes and cartilage tissue cultures from "old" and OA joints, experimental evidence is required. With regard to in vivo studies, few extensive publications are reported and they are on the same animal model. Therefore, there is the need for other investigations in other animals, such as rabbits and sheep. From a clinical point of view, some multicentric randomized and double-blind clinical trials are currently being carried out with initial promising results [40].

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